



A Non-Iterative Eigenfunction-Based Inverse Solver for PEC-Enclosed Electromagnetic Imaging

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1 Extended Abstract

For nearly a decade researchers have been interested in electromagnetic imaging within PEC-bounded enclosures [1]-[4], either out of necessity [3], for simplified modelling [4], or to investigate advantages over open-field configurations [1, 2, 4]. Within PEC enclosures, eigenfunctions provide a natural basis for electromagnetic fields and can also be used to expand unknown contrast or contrast source profiles, as previously demonstrated in a 2D TM iterative contrast source inversion (CSI) algorithm for the reconstruction of complex dielectric targets in circular systems [2]. This method made use of an underlying pixel-based discretization of the imaging domain to evaluate the required norms. More recently, we have been investigating semi-analytic, mesh-free eigenfunction formulations [5] for electromagnetic inversion within PEC enclosures, focusing on mechanisms by which to constrain the class of recoverable contrast sources through appropriately selected measurements, Green's theorem based constraints, and prior knowledge of contrast source locality.

In this work, we present a unique non-iterative scheme for direct recovery of contrast sources via a constrained eigenfunction-basis 2D TM inverse source problem. This approach exploits the one-to-one correspondence between contrast source coefficients and scattered field coefficients within the appropriate eigenfunction basis. This essentially converts the inverse source problem to a global scattered-field recovery problem. The fact that contrast sources are zero outside the imaging domain imposes constraints on the corresponding field coefficients and provides regularization. Combining the solutions for a set of interrogating transmitters allows for the contrast profile to be recovered directly in the least-square sense, an approach common to other inversion techniques such as CSI. This formulation has been tested on synthetic data for a variety of simple low-contrast targets, as well as for high-contrast synthetic biological targets. To deal with the practical design of such imaging systems, synthetic data is taken as tangential magnetic field measurements over the enclosure boundary. As will be shown, results are promising as they compare well with, and at times out-perform, a DGM-CSI algorithm [6].

References

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