

Neuromodulation by Exposure to a Pulsed Low Frequency Magnetic Field

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Abstract

Exposure to a relatively weak (100 to 1000 microTesla) low frequency (< 1000 Hz) specific pulsed magnetic field (CNP) has produced analgesia (antinociception) in snails, mice, and humans, and altered normal resting EEG in human subjects. We have also shown changes in human brain activation using fMR(BOLD) imaging due to a specific pulsed CNP exposure applied through the MR gradient coils. The alteration in brain activation corresponds to regions of interest associated with the affective processing of pain signaling.

Introduction

Neuromodulation, the alteration of neuronal activity through electrical or magnetic stimulation, is proving to become one of the most effective means of selectively altering brain and spinal cord activation for some conditions. While electrical stimulation such as deep brain stimulation (DBS) is still an extremely invasive technique, new and novel forms of magnetic stimulation leading to neuromodulation are non-invasive and hold the promise of being versatile enough for individualized therapy in the near future. CNPs have been applied to snails, mice, and humans [1-6] in previous studies and most recently a method of exposing humans to CNPs during functional magnetic resonance imaging utilizing blood oxygen level dependence (fMRI(BOLD)) has been developed with specialized MRI gradient system programming.

Methods

The CNP is an arbitrary waveform (see Figure 1, USPTO # 6,234,953 Fralex Therapeutics Inc. Toronto Ontario Canada) presented as a time-varying magnetic field normally produced through Helmholtz coils [7-8] or head coils [9]. Here we utilized the gradient coils within a Siemens Avanto 1.5 Tesla MRI system to apply a 200 microTesla (peak) magnetic field midbrain, with a 10 cm gradient to 0 microTesla CNP. In this latest study subjects were tested at their thermal pain threshold [9] on the hypothenar eminence of the hand in an fMRI(BOLD) paradigm and then exposed to either the CNP or a sham exposure while in the MRI system, and then again tested at the thermal pain threshold during the fMRI(BOLD) paradigm. The CNP or SHAM condition (no CNP) was applied for 15 min between the Pre-exposure fMRI(BOLD) thermal pain imaging session and fMRI(BOLD) thermal pain Post-exposure imaging session. Several regions of interest (ROIs) were selected for analysis relating to the affective processing of pain, including executive function (posterior cingulate (see Fig 2)) and pain processing (anterior cingulate (not shown)).

Results

Significant alteration of brain activation in the ROIs associated with pain processing and executive function were evidenced after receiving 15 min of exposure to the CNP as compared to the SHAM (Post-exposure fMRI(BOLD) signal minus Pre-exposure fMRI(BOLD) signal at $P < 0.05$) (see Fig 2 for visual comparison). Additional ROIs were likewise examined and provide significant evidence of alteration of fMRI(BOLD) signal (not shown here, see URSI GA 2008 symposium paper by Robertson et al).

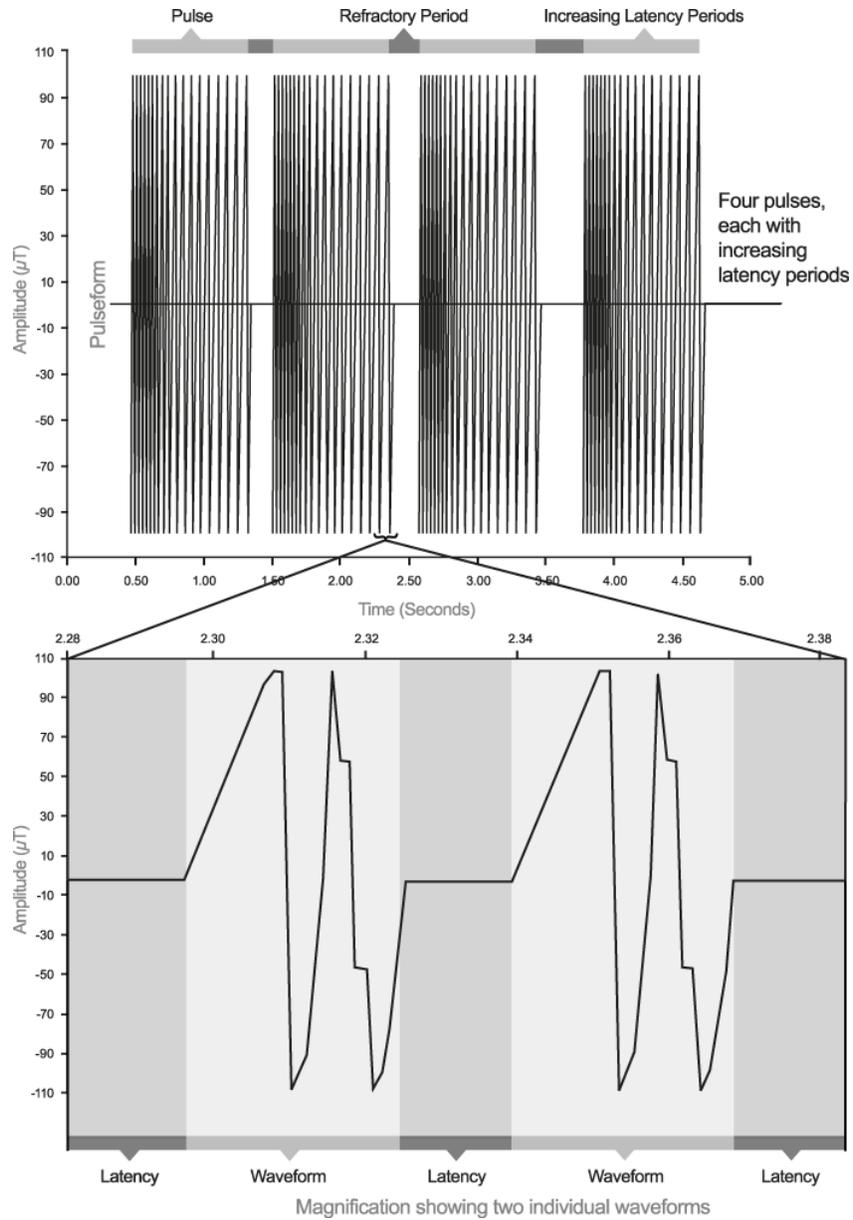


Figure 1: CNP recording (mid-brain, in non-magnetic head phantom, 100 microTesla (peak)). Each individual waveform is separated by a latency period and combined in sets to produce pulse trains containing waveforms, latency periods, and refractory periods (see USPTO #6,234,953). Reprinted with the permission of Fralex Therapeutics Inc (Toronto, Ontario, Canada).

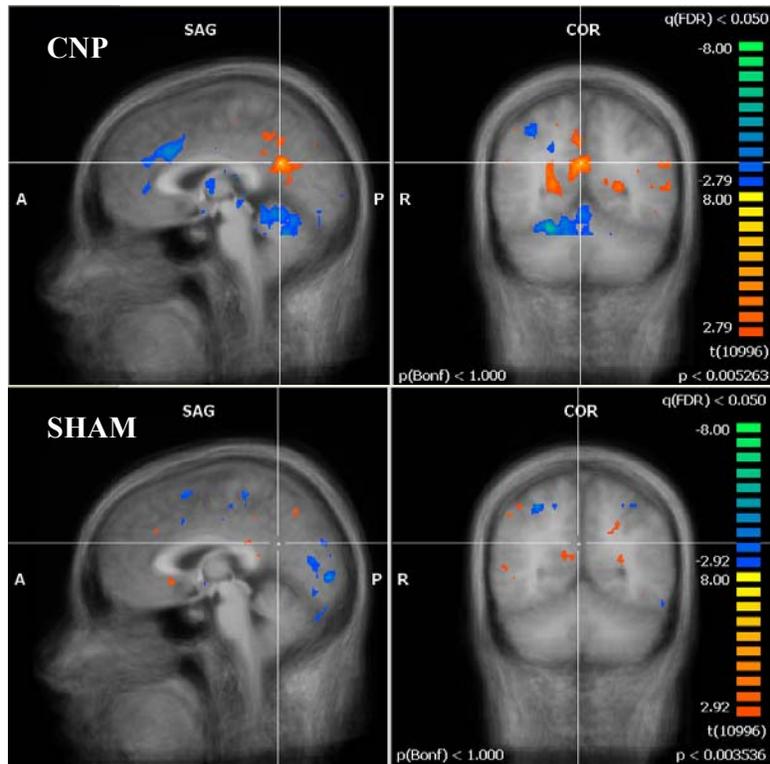


Figure 2: Posterior cingulate (N=31, CNP=14 (upper set), Sham=17 (lower set)) imaged (fMRI(BOLD)) with pre-exposure brain activation subtracted from post-exposure brain activation. All activation shown is significant ($P < 0.05$) and has been corrected for multiple tests using the FDR method (Brain Voyager). Anatomical images have been averaged for all subjects (thus the fuzzy appearance) to more accurately represent true anatomical placement within the studied group. Increases in fMRI(BOLD) signal (activation) is evidenced from yellow-red coloration, while decreases in signal are evidenced by blue-green coloration.

Discussion

Previous human studies have utilized 2m Helmholtz coil designs and head-worn coils which produce equivalent therapeutic success [9-11]. Here, the CNP was delivered within a 1.5 Tesla MRI environment, which means that the effects of the 200 microTesla CNP was evident even though there was the 1.5 Tesla static MF, the gradient MF, and the imaging RF MF produced during the protocol as well as the CNP. This leads to an intriguing hypothesis that the CNP effects are related the ‘information’ provided by the waveform, and not the MF exposure itself as a tissue-transduced non-specific MF signal, or a generalized response to MF. Further data analysis and research will explore this hypothesis.

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